

Clinical importance of remote monitoring of respiratory function

- Weakness of respiratory muscles in neurological conditions like Parkinson's Disease or Amyotrophic Lateral Sclerosis may result in dysarthria¹
- Respiratory function is key to efficient speech production and an objective measure for disease diagnosis and management
- Current clinical standard is a spirometry test²: patients exhale forcefully into a device that measures the flow of exhaled air
- Telemedicine has been gaining traction; current COVID-19 pandemic³ highlights the need to make clinical tests available to patients at home
- Unmet need for remote spirometry to allow on-demand remote monitoring of patients' respiratory function

NEMSI bridges this gap!

- NEurological and Mental health Screening Instrument (NEMSI)⁴**
 - cloud-based multimodal dialogue system that conducts automated screening interviews by engaging with conversational AI over a device of the user's choice (smartphone, tablet, laptop) from the comfort of their home
 - deployed in an automatically scalable cloud environment allowing it to serve an arbitrary number of end users at a very small cost per interaction
 - natively equipped with real-time speech and video analytics modules that extract a variety of features of direct relevance to clinicians, thus allowing for measurement of multiple subsystems (motoric, phonatory) in conjunction with lung function

Flowchart for a remote spirometry call

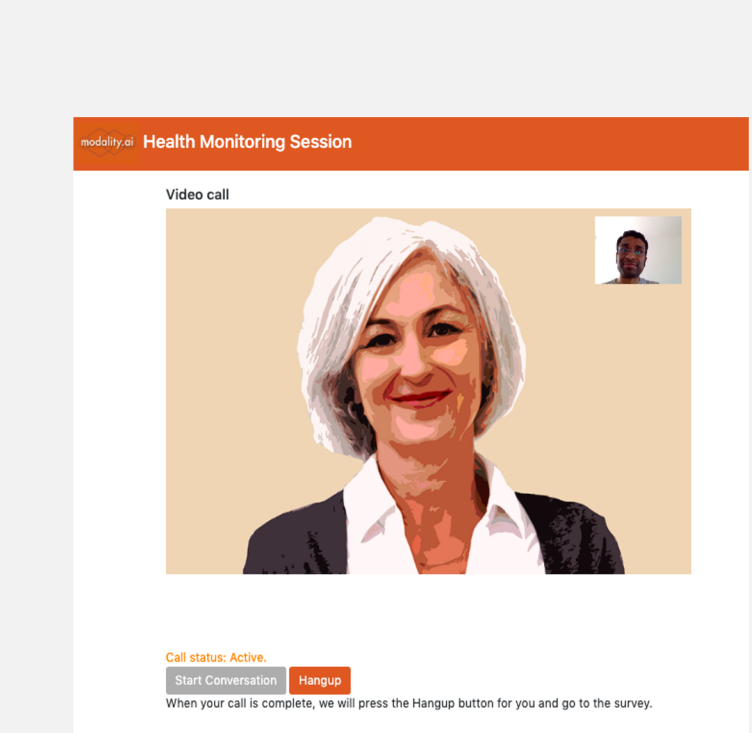
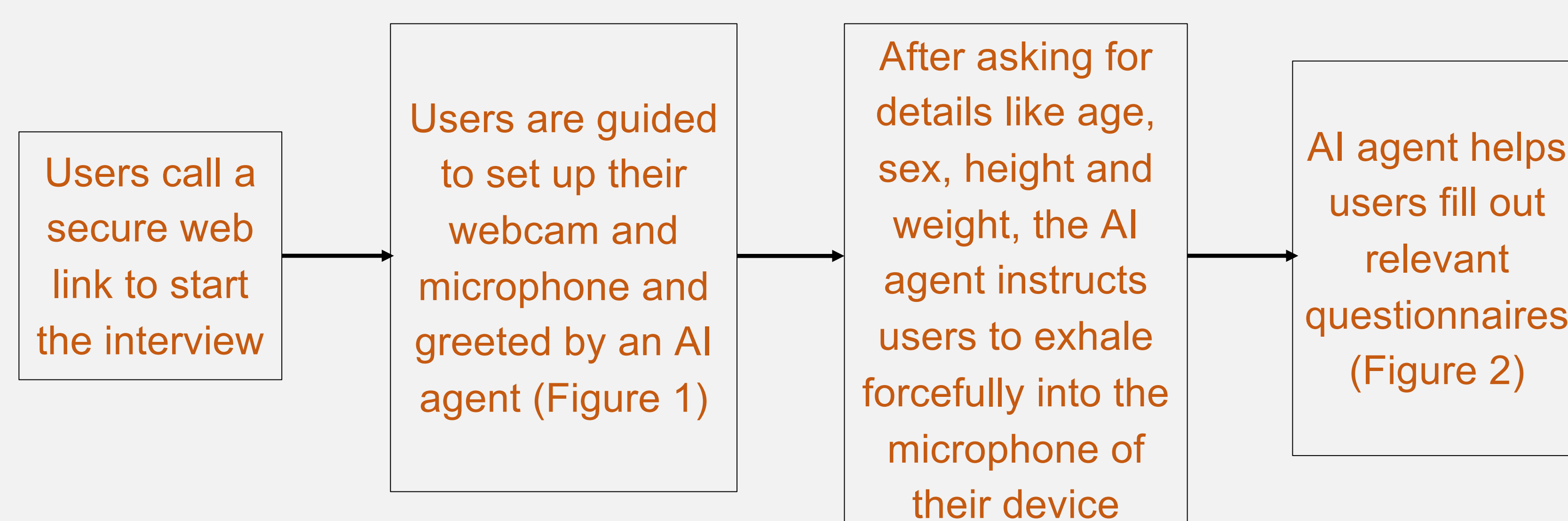


Figure 1: Example call

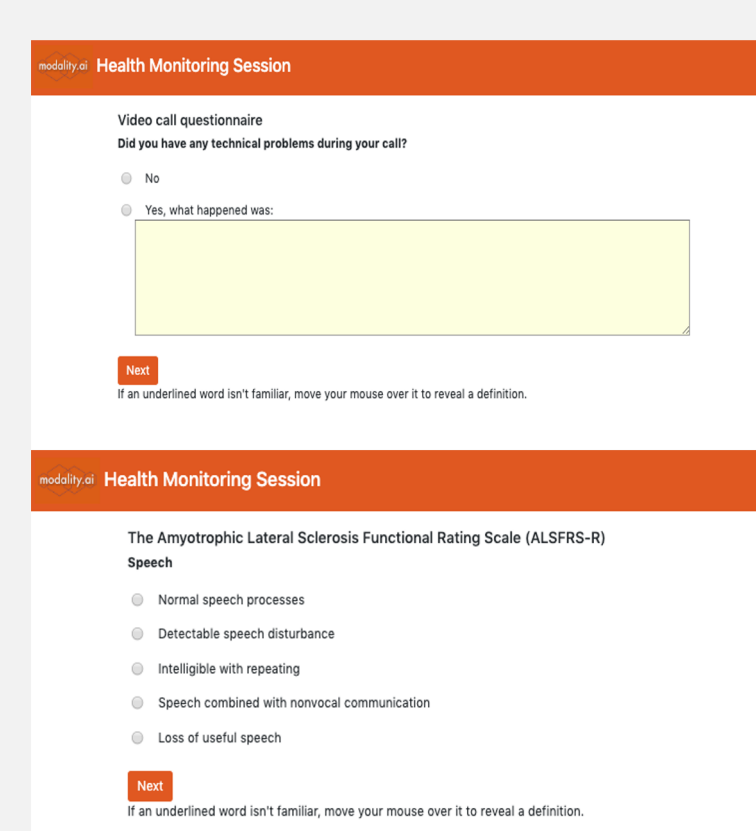


Figure 2: Questionnaires

Patient ID	Age	Sex	Height	Weight	FVC	FEV1	FEV1/FVC
1	65	F	165	70	2.5	1.5	0.6
2	70	M	180	85	3.0	2.0	0.67
3	60	F	155	65	2.0	1.2	0.6
4	75	M	175	90	3.5	2.2	0.63
5	68	F	160	75	2.8	1.8	0.64

Figure 3: Dashboard

Analytics modules extract metrics automatically

- Amplitude envelope in units of pressure (pascals) extracted from the audio signal after calculating the Hilbert envelope and adding it to the raw signal.
- Pressure at lips or $p_{lips}(t)$ is assumed to be equivalent to pressure at mic (by standardisation of mic-to-mouth distance as 2 inches or ~5cm) and flow rate at lips or $u_{lips}(t)$ is estimated as done in previous studies⁵, $u_{lips}(t) \sim 2\pi r_{lips}^2 \sqrt{2p_{lips}(t)}$ where r_{lips} is the radius of the lip aperture. Exhaled volume of air is estimated by integrating flow with respect to time.
- Measures like Forced Vital Capacity (FVC) or the total exhaled volume of air and Forced Expiratory Volume in 1 second (FEV1) and FEV1/FVC ratio extracted.
- Measures displayed on a user-friendly dashboard accessible by clinicians and researchers (Figure 3).

Analysis of metrics

- The work presented here is currently still in early stages of development and has only undergone internal testing.
- We attempted to standardise various aspects of data collection like mic type and mic-to-mouth distance.
- However, as in clinical spirometry, poor user adherence to instructions and resulting user errors are a major hurdle.
- Slow exhalation (as opposed to a forced burst) may result in an overestimation of FVC values and underestimation of FEV₁ values (see Figure 4A) whereas incomplete exhalation results in an underestimation of FEV₁ and FVC values (see Figure 4B).
- Not holding the microphone at the recommended distance causes the audio signal to be too quiet resulting in incorrect FEV₁ and FVC values but an accurate FEV₁/FVC ratio (see Figure 4C).
- In the absence of user errors, all estimated metrics fall within the range of predicted values for the user's age, sex and height (see Figure 4D) as specified in reference charts⁶.

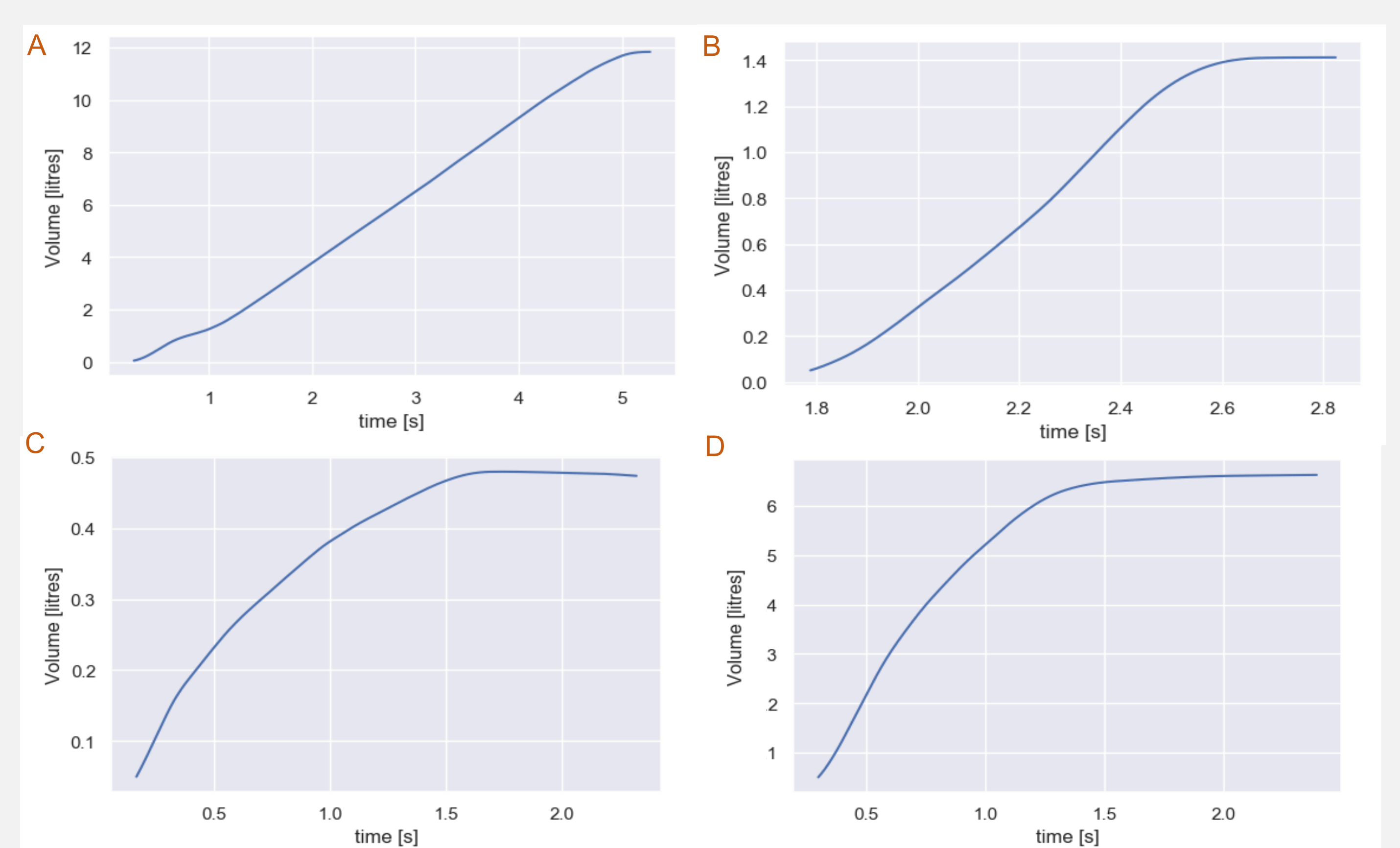


Figure 4: Volume vs Time plots (A) Slow exhalation, (B) Incomplete exhalation, (C) Microphone held far away, (D) No user errors
Note: The axes are not uniform across panels

Next steps

- Our cloud-based multimodal dialogue system provides an integrated scalable solution to remote diagnosis and monitoring of respiratory function in patients with respiratory muscle weakness and dysarthric speech.
- However, there are several limitations that need to be overcome before the solution can be implemented.
 - We look forward to working with the research community on the following points:
 - Ideas on ensuring user adherence by means of user training and intelligent feedback
 - Developing a reliable method to calibrate microphones
 - Collection of preliminary data from patient populations and healthy cohorts to validate and verify our methods.
- Remote spirometry is not a replacement for clinical spirometry but provides a valuable telehealth and telemedicine tool.

References

- Darley, F. L. et al. (1975). Motor speech disorders. Saunders.
- Townsend, M. C., & Occupational and Environmental Lung Disorders Committee. (2011). Spirometry in the occupational health setting--2011 update. Journal of occupational and environmental medicine, 53(5), 569.
- Hollander, J. E., & Carr, B. G. (2020). Virtually perfect? Telemedicine for COVID-19. New England Journal of Medicine, 382(18), 1679-1681.
- Suendermann-Oeft, D., et al. (2019, July) Proceedings of the 19th ACM International Conference on Intelligent Virtual Agents (pp. 245-247).
- Larson, E. C., et al. (2012, September). Proceedings of the 2012 ACM conference on ubiquitous computing (pp. 280-289).
- Quanjer, P. H., et al. (2012). Multi-ethnic reference values for spirometry for the 3-95-yr age range: the global lung function 2012 equations. European Respiratory Journal : 1324-1343